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ABSTRACT

Background Expired carbon dioxide (ECO₂) indicates degree of lung aeration immediately after birth. Favourable ventilation techniques may be associated with higher ECO₂ and a faster increase. Clinical condition will however also affect measured values. The aim of this study was to explore the relative impact of ventilation factors and clinical factors on ECO₂ during bag-mask ventilation of near-term newborns.

Methods Observational study performed in a Tanzanian rural hospital. Side-stream measures of ECO₂, ventilation data, heart rate and clinical information were recorded in 434 bag-mask ventilated newborns with initial heart rate <120 beats per minute. We studied ECO₂ by clinical factors (birth weight, Apgar scores and initial heart rate) and ventilation factors (expired tidal volume, ventilation frequency, mask leak and inflation pressure) in random intercept models and Cox regression for time to ECO₂ >2%.

Results ECO₂ rose non-linearly with increasing expired tidal volume up to >10 mL/kg, and sufficient tidal volume was critical for the time to reach ECO₂ >2%. Ventilation frequency around 30/min was associated with the highest ECO₂. Higher birth weight, Apgar scores and initial heart rate were weak, but significant predictors for higher ECO₂. Ventilation factors explained 31% of the variation in ECO₂ compared with 11% for clinical factors.

Conclusions Our findings indicate that higher tidal volumes than currently recommended and a low ventilation frequency around 30/min are associated with improved lung aeration during newborn resuscitation. Low ECO₂ may be used to identify unfavourable ventilation technique. Clinical factors are also associated with persistently low ECO₂ and must be accounted for in the interpretation.

INTRODUCTION

Around 3%–6% of newborns receive positive pressure ventilation at birth to facilitate transition and establish cardiorespiratory stability.^{1–3} Heart rate (HR) response is an important indicator of effective resuscitation,^{3 4} but cannot directly assess ventilation. Hooper *et al* found that expired carbon dioxide (ECO₂) indicates degree of lung aeration immediately after birth.⁵

What is known about the subject?

- Expired CO₂ (ECO₂) is low immediately after birth before the lung liquid is cleared.
- ECO₂ may serve as a marker for effective ventilations in intubated patients.

What this study adds?

- The quality of ventilations are more important than the clinical condition for measured ECO₂ during the first minutes of bag-mask ventilation in newborn resuscitation.
- Ventilation frequency around 30/min gives the highest ECO₂.
- Tidal volumes of 10–14 mL/kg are associated with the highest ECO₂ and the shortest time to reach ECO₂ >2%.

Newborn lungs are liquid filled. Before functional residual capacity is sufficiently established, gas exchange is diffusion limited.⁶ To detect ECO₂, liquid must be cleared and air must enter the alveoli. ECO₂ increases rapidly in the first minute of extrauterine life during spontaneous breathing, but slower if positive pressure ventilation is needed.^{7–9} Capnography may help identify unfavourable technique and guide ventilations during newborn resuscitation.^{10–14} There is currently insufficient evidence that ECO₂ monitoring during newborn resuscitation affects outcome.^{3 15} ECO₂ depends, in addition to ventilation, on metabolism and pulmonary circulation.¹⁶

Optimal ventilation strategies for rapidly establishing effective pulmonary gas exchange in non-breathing newborns have not been fully determined. Recent studies indicate that larger tidal volumes (V_{TE}) than the 4–8 mL/kg currently recommended may cause faster increase in HR.^{4 17 18} Guideline recommendations for ventilation frequency vary between



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the USA (40–60/min) and Europe (30/min), and evidence for any recommendation is sparse.^{19 20}

In this study, we aimed to explore the relative impact of ventilation factors (V_{TE} , frequency, mask leak and pressure) and clinical factors (birth weight (BW), Apgar scores and initial HR) on ECO_2 during bag-mask ventilation (BMV) in resuscitation of term and near-term newborn infants. Better understanding may improve interpretation of ECO_2 measurements and help determine optimal ventilation strategies.

METHODS

Study design and setting

Observational study performed between 1 March 2013 and 1 June 2017 at Haydom Lutheran Hospital, a rural Tanzanian referral hospital with 4–5000 deliveries annually. The study was part of Safer Births, a research consortium on labour surveillance and newborn resuscitation in low-income settings.^{4 21 22} Midwives and nursing students conducted most vaginal deliveries. Newborn resuscitation was mainly the responsibility of midwives.

Data collection, equipment and training

Trained non-medical research assistants observed all deliveries, documented time intervals and recorded perinatal information.² A newborn resuscitation monitor developed for research by Lærdal Global Health, Stavanger, Norway was mounted on the wall above all resuscitation tables (23). Each monitor was equipped with a self-inflating bag (230 mL standard or 320 mL Upright bag-mask; Laerdal Medical, Stavanger, Norway) and a dry-electrode ECG sensor to be easily placed around the newborns' trunk. Sensors for side-stream CO_2 (ISA; Masimo, Irvine, California, USA), pressure (Freescall semiconductor, Austin, Texas, USA) and flow (Acutronic Medical Systems, Hirzel, Switzerland) to record ECO_2 and ventilation parameters were placed between the mask and bag; the attachment device added a dead space of 1 mL. The monitors provided HR feedback. ECO_2 and ventilation parameters were not displayed.

The local newborn resuscitation procedure followed the Helping Babies Breathe (HBB) guidelines.²⁴ HBB was introduced at the study site in 2009. Midwives participated in full-day HBB courses one to two times yearly, and were educated to use clinical signs including chest rise and HR feedback to guide resuscitation. Low-dose, high-frequency skills training as described by Mduma *et al* was encouraged.²²

Formation of the cohort

We included all live-born newborns with initial HR <120 bpm who had received BMV at birth, and had available HR, ventilation and observational data (figure 1). Our research group recently showed that normal HR is around 120 bpm in the first seconds of life.²⁵ Low initial HR is a known risk factor for unfavourable outcome.²¹ Newborns who received BMV but had HR ≥ 120 bpm

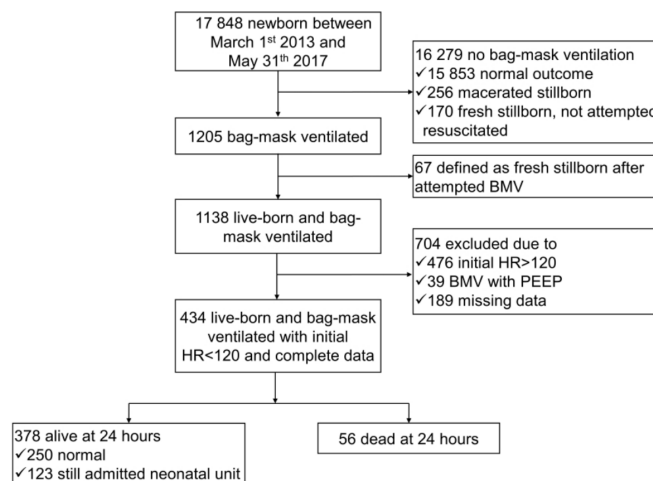


Figure 1 Overall newborn mortality at Haydom Hospital during the study period was 31 per thousand births. Among these, 28 were defined as still births, 13 fresh and 15 macerated. BMV, bag-mask ventilation; HR, heart rate; PEEP, positive end-expiratory pressure.

at onset of recording were excluded as these are likely different in pathophysiology and prognosis. Newborns randomised to receive BMV with positive end-expiratory pressure (PEEP) valve in a parallel intervention study were excluded due to potential impact of PEEP on ECO_2 .

Outcome and covariates

The primary outcome was the maximum percentage of CO_2 in expired air per ventilation. Secondary outcome was time to $ECO_2 > 2\%$ from the first BMV.

To characterise assisted ventilations ('ventilation factors'), we used repeated measures for expired V_{TE} , ventilation frequency, peak inflating pressure (PIP) and mask leak smoothed as means per five ventilations. The threshold to detect a ventilation was set to PIP >5 mbar.

As markers of clinical condition ('clinical factors'), we used the initial HR and 5 min Apgar score. Initial HR was defined as the mean of the first five HR values recorded for each newborn. The 5 min Apgar score was selected due to established association with asphyxia.²⁶ In a sensitivity analysis, we substituted Apgar score at 5 min with 1 min because 5 min score may be affected by treatment.

We also included BW and time as covariates. In the primary analyses, within the first 5 min of ventilation, time was recorded from the first detected ventilation. In the secondary analyses, per ventilation sequences, time was recorded from the first detected ventilation per sequence. We defined a ventilation sequence as continuous BMV with <5 s pause between two ventilations.

$V_{TE} > 30$ mL/kg were considered unlikely to be correct measurements and were excluded. We also excluded individual observations with ventilation frequency >120/min as this is twice the upper limit of recommended ventilation frequency.

Table 1 Baseline characteristics and covariates

		All newborns (n=17 848)*	Included newborns (n=434)*	ICC†
Delivery mode	Caesarean section	3937 (23%)	215 (50%)	–
	Standard vaginal	13 331 (76%)	194 (45%)	–
	Breech	162 (0.9%)	24 (6%)	–
	Vacuum	39 (0.2%)	1 (0.2%)	–
	Other	14 (0.1%)	–	–
Females		8167 (47%)	168 (39%)	–
Gestational age (weeks)		38 (37–40)	38 (37–40)	–
Gestational age <36 weeks		594 (3.3%)	29 (7%)	–
Birth weight (g)		3248 ± 535	3074 ± 593	–
Apgar 1 min		9 (9–9)	6 (5–7)	–
Apgar 5 min		10 (10–10)	10 (8–10)	–
First detected heart rate (bpm)		–	73 ± 21	–
Time from birth to first ventilation (s)		–	112 (78–158)	–
Time from first to last ventilation (s)		–	184 (80–394)	–
Time to ECO ₂ >2% (s)		–	10.0 (3.1–34.9)‡	–
No of ventilation sequences		–	5 (2–8)	–
Duration of ventilation sequences (s)		–	29 ± 46§ / 18 (11 - 30)¶	0.15
Expired volume, V _{TE} (mL/kg)		–	7.9 ± 6.4§ / 6.7 (4.1–11.0)¶	0.52
Ventilation frequency (BMVs/min)		–	52 ± 24§ / 47 (38–65)¶	0.62
Mask leak (%)¶		–	44 ± 29§ / 40 (25–59)¶	0.40
Peak inflation pressure (mbar)¶		–	35 ± 11§ / 38 (25–60)¶	0.54
ECO ₂ (% of expired air) ¶		–	2.9 ± 2.2§ / 2.9 (1.3–4.1)¶	0.50
Max ECO ₂ in first 5 min of BMV		–	7.2 ± 2.8	–
Initial ECO ₂		–	0.9 (0.3–3.3)	–

*Frequencies are given in the form of n (%), parameters with skewed distributions are given as median (25th quartile, 75th quartile), normally distributed parameters as mean±SD. For ventilation factors with repeated measurements per newborn, we report both means calculated by unconditional random intercept analysis and medians of medians.

†ICC—intercorrelation coefficient: proportion of total variance assigned to variance between patients.

‡Newborns who had ECO₂ >2% in the first ventilation (n=113) or did not reach threshold (n=23) not included.

§Mean in first 5 min of BMV, SD is given as $\sqrt{\text{total variance}}$ where the total variance is the sum of variance between and within patients.

¶Median of medians in first 5 min of BMV.

BMV, bag-mask ventilation; ECO₂, expired carbon dioxide.

Statistical analyses

For cohort and data description, we report percentages, means with SD or medians with IQRs, as appropriate (table 1). For ventilation parameters, we include intercorrelation coefficients due to variation both within and between patients.

We fitted random intercept regression models to study changes in ECO₂ by variations in clinical and ventilation factors for newborns who received BMV. Associations with ECO₂ were not linear for all covariates, thus we performed log transformation for time, and included a quadratic term for V_{TE} and PIP guided by Akaike's information criteria and inspection of the residuals. To compare the effect of covariates measured on different scales, we report beta values per standardised units ((x–mean)/SD) in addition to the measured scale for each covariate and coefficients of determination (R² values).

R² was calculated as the proportional reduction in prediction error variance comparing models with and without the covariate of interest.²⁷ For closely correlated parameters, we excluded both parameters simultaneously.

The primary analysis was performed in the first 5 min of BMV. Second, we compared the effects per ventilation sequence for newborns who had three or more sequences lasting for more than 10s to evaluate build-up effects and the impact of pauses. We used Cox regression to study predictors for time from first BMV until ECO₂ reached 2% (≈2 kPa or 15 mm Hg at sea level). ECO₂ threshold was set at 2% as this corresponds well with changes on the colorimetric CO₂ detectors¹¹ and the ECO₂ level found to be most predictive for HR >60 bpm.²⁸ Kruskal-Wallis test was used to compare clinical and ventilation factors in three groups of infants differing by when ECO₂ >2% was achieved: never, during ventilation or spontaneously.

Data analysis was performed using MATLAB (MathWorks, Natick, Massachusetts, USA) and Stata SE V.14.2 (StataCorp, College Station, Texas, USA). We used a purposeful selection approach to build regression models; only significant covariates ($p < 0.05$) were included in the final models.

Patient and public involvement

The study was performed in an area with high illiteracy rate, and patients and public were not directly involved in the planning of the study. Oral feedback from patients and personnel were taken into account for solving practical issues concerning data collection during the study period.

Ethical considerations

All women were informed, but consent was not considered necessary by the ethical committees.

RESULTS

During the study period, 17 484 babies were born in the hospital; 6.9% received BMV (figure 1). Among 434 included newborns, 400 had a minimum of one ventilation sequence that lasted for more than 10s (baseline data in table 1).

Predictors of ECO_2 during first 5 min

Both clinical and ventilation factors were significantly associated with ECO_2 , but ventilation explained substantially more of the variance than clinical factors (R^2 30.8% vs 10.9%); V_{TE} was the strongest single predictor (table 2). The association between V_{TE} and ECO_2 was positive and close to linear for $V_{TE} < 10$ mL/kg, levelling off at 10–20 mL/kg and negative > 20 mL/kg (figure 2A). Mask leak and V_{TE} were negatively correlated, and together explained 23% of the variance in ECO_2 . Low ventilation frequency around 30/min was associated with

Table 2 Linear random intercept model for predictors of expired carbon dioxide (ECO_2) in the first 5 min of bag-mask ventilation

Covariates	Univariate model*			Multivariate model			
	Coefficient (95% CI)	P value	R^2 (%)	Coefficient (95% CI)	P value	R^2 (%)	R^2 (%)
ECO_2 (unconditional)	2.90 (2.75 to 3.05)						
Ventilation characteristics							
Expired tidal volume (V_{TE})	0.37 (0.33 to 0.42)	<0.001	19.3	0.32 (0.27 to 0.37)	<0.001	23.1†	30.8
Per mL/kg increase	2.37 (2.10 to 2.65)			2.02 (1.71 to 2.33)			
Per standardised unit							
$(V_{TE})^2$		<0.001			<0.001		
Per 100 (mL/kg) ² increase	-0.86 (-1.0 to 0.7)			-0.78 (-0.9 to -0.6)			
Per standardised unit	-1.29 (-1.53 to -1.06)			-1.17 (-1.40 to -0.94)			
Mask leak		<0.001	16.1		0.009		
Per 10% increase	-0.30 (-0.33 to -0.27)			-0.056 (-0.098 to -0.014)			
Per standardised unit	-0.85 (-0.87 to -0.84)			-0.16 (-0.29 to 0.42)			
Ventilation frequency		<0.001	7.5		<0.001	16.1‡	
Per 10 bpm increase	-0.17 (-0.23 to -0.11)			-0.16 (-0.19 to -0.12)			
Per standardised unit	-0.40 (-0.55 to -0.26)			-0.37 (-0.45 to -0.28)			
Peak inflation pressure (PIP)		0.001	1.1		0.008	-0.3	
Per 10 mbar increase	0.41 (0.16 to 0.67)			0.24 (0.064 to 0.29)			
Per standardised unit	0.46 (0.18 to 0.75)			0.27 (0.071 to 0.46)			
$(PIP)^2$		<0.001			<0.001		
Per 10 mbar ² increase	-0.60 (-0.87 to -0.33)			-0.47 (-0.64 to -0.29)			
Per standardised unit	-0.61 (-0.88 to -0.33)			-0.47 (-0.65 to -0.29)			
Clinical factors							
Birth weight	0.78 (0.51 to 1.04)	<0.001	4.4	0.81 (0.58 to 1.03)	<0.001	6.8	10.9
Per kg increase	0.46 (0.30 to 0.62)			0.48 (0.34 to 0.61)			
Per standardised unit							
Initial heart rate	0.081 (0.012 to 0.15)	0.022	0.6	0.089 (0.034 to 0.14)	0.002	1.3	
Per 10 bpm increase	0.17 (0.024 to 0.31)			0.19 (0.070 to 0.30)			
Per standardised unit							
5 min Apgar score	0.054 (-0.021 to 0.13)	0.16	0.3	0.14 (0.068 to 0.22)	<0.001	2.9	
Per one unit increase	0.11 (-0.043 to 0.26)			0.29 (0.14 to 0.44)			
Per standardised unit							
Log2 of time in seconds	0.33 (0.28 to 0.38)	<0.001	2.0	0.15 (0.12 to 0.19)	<0.001	0.9	0.9
Per unit increase	0.64 (0.54 to 0.73)			0.29 (0.23 to 0.36)			
Per standardised unit							
Random-effects parameters				Var (_cons) 1.53 (1.31 to 1.77)§			
				Var (Residual) 1.53 (1.34 to 1.74)			
				ICC 0.50			

*Intercorrelation coefficient (ICC) varied between 0.47 and 0.56 for all covariates.

† V_{TE} and mask leak were correlated (Spearman's rho -0.65). Excluding V_{TE} from the model, beta value for mask leak decreased from -0.056 (-0.098 to -0.014) to -0.28 (-0.31 to -0.24). R^2 for V_{TE} alone excluding mask leak from the model was 21.9%. R^2 for mask leak excluding V_{TE} was 17.1%.

‡Interaction term for V_{TE} and frequency was significant with beta=-0.015 (-0.020 to -0.0091), $p < 0.001$, the model is displayed without this term for interpretability. V_{TE} and frequency were still significant in the model including the interaction term.

§ R^2 for the total model: 36.6%.

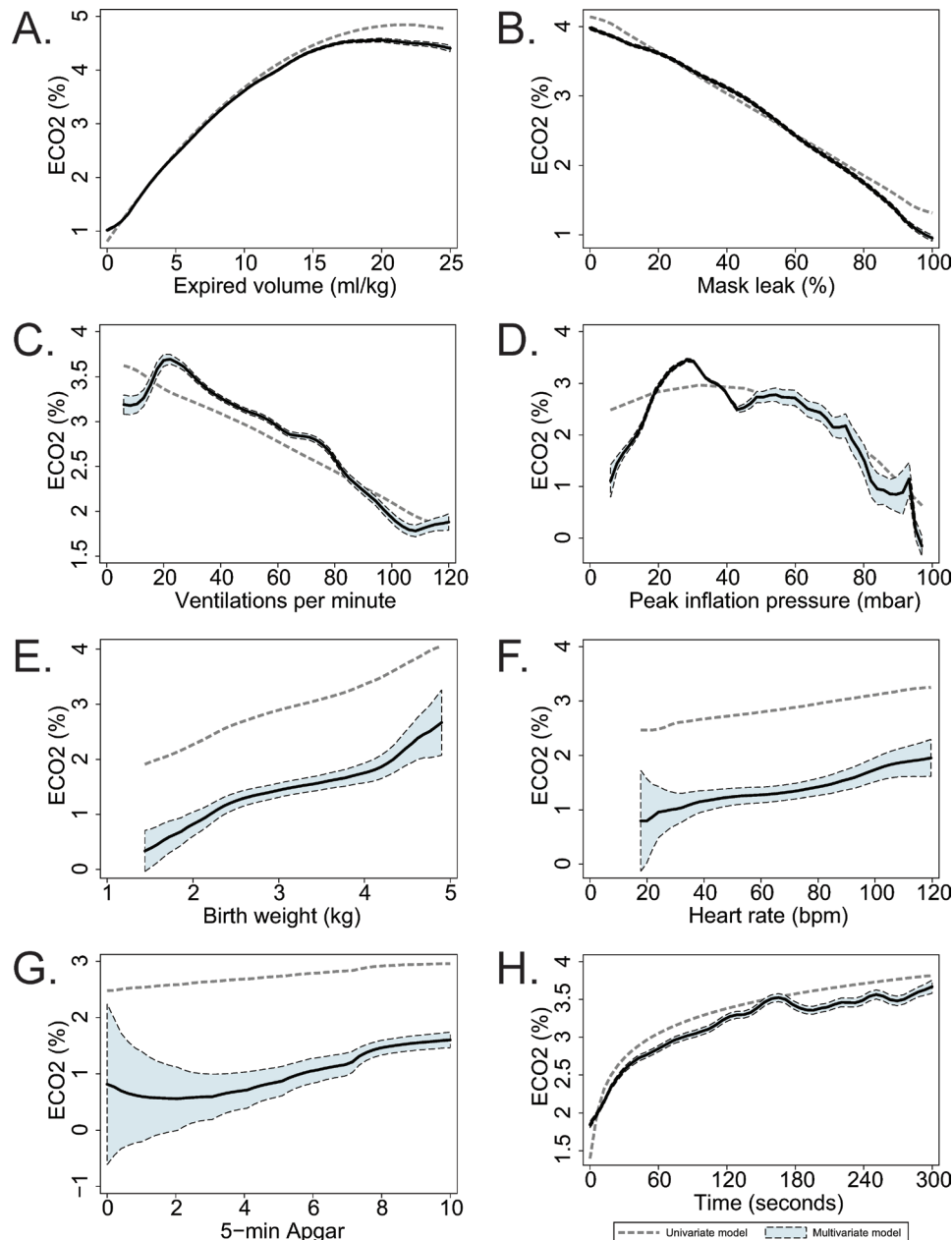


Figure 2 ECO_2 by covariates. Smoothed local polynomial plots for predicted values of expired carbon dioxide (ECO_2) per covariate in univariate (dashed, grey line) and multivariate model (solid, black line). The graphs display ECO_2 versus (A) expired tidal volume (V_{TE} , mL/kg), (B) mask leak (percentage leak), (C) ventilation frequency (ventilations per minute), (D) peak inflation pressure (PIP, mbar), (E) birth weight (kg), (F) initial heart rate (beats per minute), (G) 5 min Apgar score and (H) time (seconds). Table 2 display effect measures (beta coefficients), p values and explained variance (R^2) for the regression models.

the highest ECO_2 (figure 2C). PIP <15 or >60 mbar were associated with low ECO_2 (figure 2D). ECO_2 increased rapidly in the first minute of BMV, V_{TE} increased and mask leak decreased simultaneously (figure 3). BW and initial HR were positively associated with ECO_2 in univariate and multivariate models, 5 min Apgar score only in the multivariate model (table 2, figure 2E–G).

Predictors for ECO_2 by ventilation sequence

Analysing the first three ventilation sequences with duration >10s (online supplementary appendix table S1 A–C) gave similar results as the primary analysis, with

V_{TE} as the strongest predictor. ECO_2 increased significantly with time in the first two ventilation sequences, but not in the third (online supplementary appendix figure S1).

Predictors for time to reach threshold

The Cox model found higher V_{TE} up to 14 mL/kg to be associated with shorter time to reach $\text{ECO}_2 >2\%$ (table 3). Higher 5 min Apgar score, initial HR, BW and PIP were also associated with shorter time to reach $\text{ECO}_2 >2\%$.

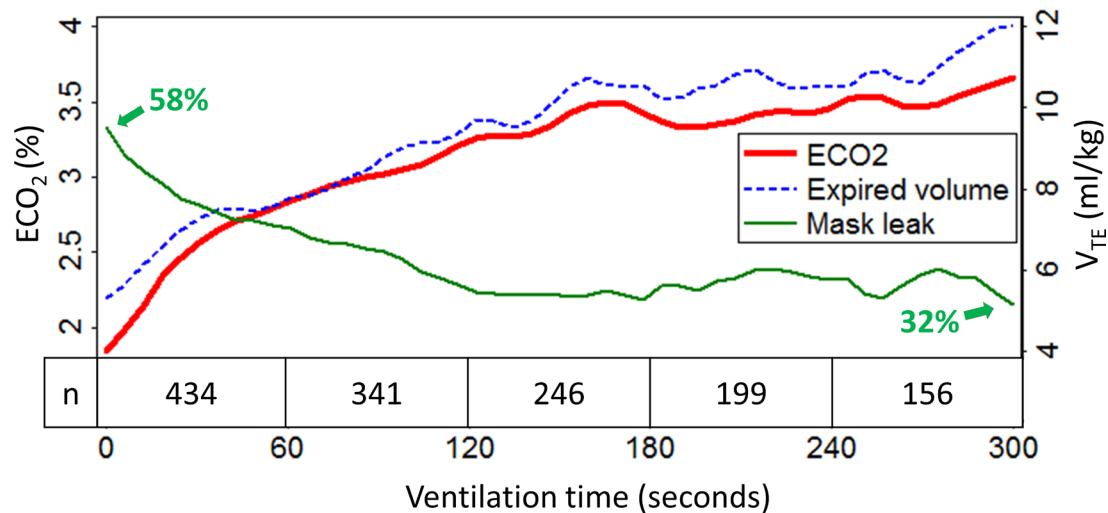


Figure 3 Change in expired carbon dioxide (ECO_2), expired volume and mask leak by time the figure illustrates trends for changes in ECO_2 (red, solid line), V_{TE} (blue, dashed line) and mask leak (green, dashed line) by time. The graphs are smoothed local polynomial plots. The integrated table displays the number of newborns (n) who received ventilations in each minute since start of ventilations.

Interactions and stratified analyses

In the primary analysis, we found a significant interaction for V_{TE} and frequency. We found no relevant differences stratified by $\text{BW} \geq 2500$ g versus < 2500 g, initial HR ≥ 60 versus < 60 bpm, vaginal delivery versus Caesarean

section or for newborns ventilated within versus after 60s from birth (data not shown). Substituting V_{TE} and ventilation frequency with respiratory minute volume, we found a non-linear positive association between ECO_2 and minute volumes (online supplementary appendix

Table 3 Cox regression for time to $\text{ECO}_2 > 2\%$ (n=321)*

	Univariate model		Multivariate model†‡	
	Hazard Ratio (95% CI)	P value	Hazard Ratio (95% CI)	P value
Expired tidal volume (V_{TE})				
Per 1 mL/kg increase	1.18 (1.11 to 1.24)	<0.001	1.22 (1.15 to 1.29)	<0.001
Per standardised unit	1.33 (1.18 to 1.50)		3.75 (2.56 to 5.48)	
(V_{TE})²§				
Per unit increase	0.99 (0.99 to 0.99)	<0.001	0.99 (0.99 to 1.0)	<0.001
Per standardised unit	1.16 (1.02 to 1.31)		0.34 (0.22 to 0.52)	
Peak inflation pressure				
Per 10 mbar increase	1.24 (1.15 to 1.35)	<0.001	1.32 (1.21 to 1.43)	<0.001
Per standardised unit	1.28 (1.17 to 1.40)		1.36 (1.24 to 1.50)	
Birth weight				
Per kg increase	1.32 (1.09 to 1.59)	0.004	1.42 (1.17 to 1.72)	0.001
Per standardised unit	1.18 (1.05 to 1.32)		1.23 (1.10 to 1.38)	
Initial heart rate				
Per 10 bpm increase	1.08 (1.02 to 1.14)	0.004	1.08 (1.02 to 1.14)	0.006
Per standardised unit	1.18 (1.05 to 1.32)		1.17 (1.05 to 1.30)	
Apgar at 5 min				
Per unit increase	1.10 (1.04 to 1.16)	0.001	1.17 (1.11 to 1.24)	<0.001
Per standardised unit	1.23 (1.09 to 1.38)		1.42 (1.25 to 1.61)	

*Among n=434 included newborns, 113 were censored before analysis due to $\text{ECO}_2 > 2\%$ in the first ventilation, 321 were included in the Cox regression, 23 never reached $\text{ECO}_2 > 2\%$.

†Hazard Ratios were not proportional for V_{TE} alone, including a quadratic term gave acceptable fit in the multivariate model.

‡Mask leak was significant ($p < 0.001$) in univariate model, but not in multivariate model ($p = 0.26$) including V_{TE} due to correlation with volume. Taking V_{TE} out of the model, mask leak was significant with $p < 0.001$, Hazard Ratio 0.89 (0.86 to 0.93) per 10% increase.

§Ventilation frequency was not significant with $p = 0.63$ in the univariate and $p = 0.18$ in the multivariate Cox model and was omitted from the final models.

Table 4 Comparison of groups by time to threshold $\text{ECO}_2 > 2\%$

	Category of time to $\text{ECO}_2 > 2\%$			Kruskal-Wallis test *
	A: $\text{ECO}_2 > 2\%$ in first ventilation	B: $\text{ECO}_2 > 2\%$ during ventilation	C: $\text{ECO}_2 > 2\%$ never achieved	
n	113	298	23	–
Expired tidal volume, V_{TE} (mL/kg)	7.3 (4.3–11.3)	4.2 (1.9–7.4)	2.9 (1.0–5.0)	<0.001*
Mask leak (%)	41 (25–60)	55 (36–43)	78 (44–93)	<0.001†
Ventilation frequency (per minute)	45 (33–61)	48 (38–69)	64 (46–73)	0.009‡
Peak inflation pressure (mbar)	35 (31–39)	36 (31–39)	33 (25–38)	0.16
Minute volume (mL/kg per minute)	325 (171–553)	201 (82–421)	154 (51–406)	<0.001§
Birth weight (kg)	3.2 (2.9–3.5)	3.1 (2.7–3.4)	2.9 (2.6–3.2)	<0.001¶
First detected heart rate (bpm)	70 (59–94)	67 (56–85)	77 (59–83)	0.15
Apgar 1 min	7 (6–7)	6 (5–7)	5 (5–7)	<0.001**
Apgar 5 min	10 (8–10)	10 (8–10)	9 (7–10)	0.19
Time from first to last ventilation (s)	126 (63–258)	217 (95–458)	66 (22–130)	<0.001††

All values are medians (IQR). For ventilation factors, we used median per group of medians per newborn within the first 30 s of ventilation. Kruskal-Wallis test was performed to rank medians. The column shows p values for comparison of all three groups, p values for significant differences between groups compared in pairs are given as footnotes.

* V_{TE} : A≠B (p<0.001), A≠C (p<0.001), B≠C (p=0.07).

†Mask leak: A≠B (p<0.001), A≠C (p<0.001), B≠C (p=0.04).

‡Ventilation frequency: A≠B (p=0.02), A≠C (p=0.008), B≠C (p=0.07).

§Minute volume: A≠C (p=0.009), B≠C (p<0.001).

¶Birth weight: A≠B (p<0.001), A≠C (p=0.010).

**Apgar at 1 min: A≠B (p<0.001), A≠C (p=0.017).

††Time from first to last ventilation: A≠B (p=0.023), A≠C (p<0.001), B≠C (p>0.001).

table S2). Substituting 5 min Apgar scores with 1 min scores did not affect the main conclusions.

Other analyses

Table 4 groups included newborns in three: (A) $\text{ECO}_2 > 2\%$ at onset of BMV, (B) reached $\text{ECO}_2 > 2\%$ during BMV and (C) never reached $\text{ECO}_2 > 2\%$. Group A had significantly higher BW, Apgar scores and V_{TE} and lower mask leak and ventilation rate in the first 30 s of ventilations compared with groups B and C. We found no significant differences in the clinical parameters between group B and C. However, infants in group C were ventilated with higher frequencies, had more mask leak and had lower V_{TE} in the first 30 s of BMV.

DISCUSSION

In this large observational study, ventilation factors were stronger predictors for ECO_2 than clinical markers of asphyxia during initial resuscitation of term and near-term newborns. $V_{\text{TE}} > 10 \text{ mL/kg}$, low mask leak and a ventilation frequency around 30/min were associated with the highest ECO_2 .

Simultaneous collection of ventilation parameters and observation of clinical factors in a large sample of newborns allowed for analyses considering both clinical differences and quality of delivered ventilations. The main findings were replicated in alternative statistical models. The major burden of death and morbidity due to neonatal asphyxia occurs in low-income countries.²⁹ Even if the midwives' ventilation skills may not

be representative for all places, the physiological factors affecting ventilation parameters and ECO_2 must be expected to be similar for newborns all over the world. High baseline morbidity is more likely to strengthen than hide associations with clinical factors. We do not find obvious reasons limiting the validity of the main findings in a global context.

As in any observational study, our results may be affected by unmeasured or residual confounding. It is likely that subtle interactions occurred between clinical and ventilation factors due to variations in lung compliance and muscle tone. The first detected HR defined as 'initial HR' was collected with variable delay after birth depending on when the HR sensor was applied. Apgar scores are subjective measures, and interobserver variability large.^{26 30} Measures of umbilical artery pH, base excess or lactate are more objective to assess degree of asphyxia, but were not available at the study site.

We propose that ventilation characteristics associated with higher and a faster increase in ECO_2 during initial BMV are favourable to quickly establish effective gas exchange. The observed close association between V_{TE} and ECO_2 supports studies pointing to ECO_2 as an indicator of lung aeration immediately after birth.^{5 6} An increase in ECO_2 with increasing minute volumes, different from later in life, further strengthens the theory that ECO_2 is diffusion limited during initial ventilation of fluid-filled newborn lungs.³¹ As we observed an increase in ECO_2 for V_{TE} 10–20 mL/kg, and shorter time to reach $\text{ECO}_2 > 2\%$ up to 14 mL/kg, we speculate that higher V_{TE} than

the commonly recommended 4–8 mL/kg may promote a faster lung aeration. Two other studies from our group found a positive relationship between delivered V_{TE} and HR, with the most rapid increase in HR during BMV at volumes around 10 mL/kg.^{4 17} Larger V_{TE} may be needed during BMV than in intubated patients to compensate for upper airway distension.³²

We found that ventilation frequency was negatively associated with ECO_2 , suggesting less effective lung aeration at high frequencies. Highest observed ECO_2 at ventilation frequencies around 30/min points to inflation rates in the lower range of recommended values as potentially more favourable, as suggested by the European resuscitation guidelines.^{19 20}

Several authors have proposed that capnography may serve as feedback to identify airway obstruction during newborn resuscitation.^{10 13 33} Our findings partly support this. Low ECO_2 associated with high PIP may be due to obstructed airway or low lung compliance. Mask leak and PIP effects were substantially reduced in our models when adjusting for V_{TE} , likely because they mainly worked through V_{TE} modifications. We do not see obvious ways to discriminate between airway obstruction and liquid-filled lungs as explanation for low ECO_2 before higher levels have been observed.³⁴ Stronger positive linear association between PIP and ECO_2 in the first ventilation sequence compared with later sequences supports a need for higher opening pressure during initial inflations.³⁵

We observed a fast ECO_2 increase in the first minute of ventilation. This is line with previous studies indicating a gradual lung aeration.^{7–9} Efforts to improve ventilation, like clearing the airway and reducing mask leak, probably contributed to ECO_2 increase over time. Reduced ECO_2 after ventilation pauses suggests re-entry of lung liquid and supports a recommendation for continuous, effective ventilation to non-breathing newborns.¹⁸

The process of lung aeration has been found to be slower during BMV than in spontaneously breathing newborns.^{8 9 36 37} Newborns with gasping or spontaneous breaths before initiation of BMV have already started the lung-aeration process. This may explain higher initial ECO_2 in newborns with higher Apgar scores. Moreover, larger newborns may have higher respiratory drive and better reserves to handle complications during labour despite low initial HR and low Apgar scores, explaining the positive association between ECO_2 and BW.

Significant but weak negative associations found between Apgar scores, initial HR and ECO_2 underline that severely compromised circulation may cause persistently low ECO_2 .^{16 28} Waste of valuable time trying to improve correctly performed ventilations based on ECO_2 feedback may be a pitfall. To measure V_{TE} in combination with ECO_2 may reduce this risk.^{36 38}

Our findings indicate that somewhat higher V_{TE} than currently recommended and a low ventilation frequency may be favourable during bag-mask ventilation of term and near-term infants at birth. However, this is an observational study and long-term outcomes have not been

studied. Near-term newborns have more mature and less vulnerable lungs than premature infants, and asphyxia is often the cause when they do not start breathing spontaneously.³⁹ Still, the optimal V_{TE} needed to balance fast establishment of adequate ventilation to avoid brain damage against the risk for lung injury remains unclear.^{6 40} Our findings alone are not sufficiently strong to change guideline recommendations, but may provide background information for future randomised studies of V_{TE} , ventilation frequency and the use of ECO_2 feedback during newborn resuscitation.

CONCLUSIONS

Ventilation factors are important predictors for ECO_2 during the first minutes of bag-mask ventilation in newborn resuscitation. V_{TE} of 10–14 mL/kg and ventilation frequency around 30/min are associated with the highest ECO_2 , and the shortest time to reach $ECO_2 > 2\%$. Low ECO_2 may be useful to detect inefficient ventilation. Low BW, HR and Apgar scores are also associated with low ECO_2 , and this must be accounted for in the interpretation.

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Competing interests JE is an employee of Laerdal Medical. JL is married to an employee at Laerdal Global Health.

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REFERENCES

- Wall SN, Lee ACC, Niermeyer S, *et al.* Neonatal resuscitation in low-resource settings: what, who, and how to overcome challenges to scale up? *Inte J Gynecol Obst* 2009;107(Supplement):S47–64.
- Ersdal HL, Mduma E, Svensen E, *et al.* Early initiation of basic resuscitation interventions including face mask ventilation may reduce birth asphyxia related mortality in low-income countries. *Resuscitation* 2012;83:869–73.
- Perlman JM, Wyllie J, Kattwinkel J, *et al.* Part 7: neonatal resuscitation: 2015 international consensus on cardiopulmonary resuscitation and emergency cardiovascular care science with treatment recommendations. *Circulation* 2015;132(16 Suppl 1):S204–41.
- Linde JE, Schulz J, Perlman JM, *et al.* The relation between given volume and heart rate during newborn resuscitation. *Resuscitation* 2017;117:80–6.
- Hooper SB, Fouras A, Siew ML, *et al.* Expired CO₂ levels indicate degree of lung aeration at birth. *PLoS One* 2013;8:e70895.
- Hooper SB, Siew ML, Kitchen MJ, *et al.* Establishing functional residual capacity in the non-breathing infant. *Semin Fetal Neonatal Med* 2013;18:336–43.
- Schmölzer GM, Hooper SB, Wong C, *et al.* Exhaled carbon dioxide in healthy term infants immediately after birth. *J Pediatr* 2015;166:844–9.
- Palme-Kilander C, Tunell R, Chiwei Y. Pulmonary gas exchange immediately after birth in spontaneously breathing infants. *Arch Dis Child* 1993;68:6–10.
- Palme-Kilander C, Tunell R. Pulmonary gas exchange during facemask ventilation immediately after birth. *Arch Dis Child* 1993;68:11–16.
- Leone TA, Lange A, Rich W, *et al.* Disposable colorimetric carbon dioxide detector use as an indicator of a patent airway during noninvasive mask ventilation. *Pediatrics* 2006;118:e202–4.
- Hawkes GA, Kelleher J, Ryan CA, *et al.* A review of carbon dioxide monitoring in preterm newborns in the delivery room. *Resuscitation* 2014;85:1315–9.
- Mizumoto H, Iki Y, Yamashita S, *et al.* Expiratory CO₂ as the first sign of successful ventilation during neonatal resuscitation. *Pediatr Int* 2015;57:186–8.
- van Os S, Cheung P-Y, Pichler G, *et al.* Exhaled carbon dioxide can be used to guide respiratory support in the delivery room. *Acta Paediatr* 2014;103:796–806.
- Schmolzer GM, Morley CJ, Davis PG. Respiratory function monitoring to reduce mortality and morbidity in newborn infants receiving resuscitation. *The Cochrane Database of Systematic Reviews* 2010;9.
- Kong JY, Rich W, Finer NN, *et al.* Quantitative end-tidal carbon dioxide monitoring in the delivery room: a randomized controlled trial. *J Pediatr* 2013;163:104–8.
- Triilo G, Planta Mvon, Kette F. ETCO₂ monitoring during low flow states: clinical aims and limits. *Resuscitation* 1994;27:1–8.
- Thallinger M, Ersdal HL, Francis F, *et al.* Born not breathing: a randomised trial comparing two self-inflating bag-masks during newborn resuscitation in Tanzania. *Resuscitation* 2017;116:66–72.
- Foglia EE, Te Pas AB. Effective ventilation: the most critical intervention for successful delivery room resuscitation. *Semin Fetal Neonatal Med* 2018;23:340–6.
- AHA. Web-based Integrated 2010 & 2015 American Heart Association Guidelines for Cardiopulmonary Resuscitation and Emergency Cardiovascular Care, Part 13: Neonatal Resuscitation 2010 and 2015. Available: <https://eccguidelines.heart.org/index.php/circulation/cpr-ecc-guidelines-2/part-13-neonatal-resuscitation/>
- Wyllie J, Bruinenberg J, Roehr CC, *et al.* European Resuscitation Council guidelines for resuscitation 2015: section 7. Resuscitation and support of transition of babies at birth. *Resuscitation* 2015;95:249–63.
- Linde JE, Perlman JM, Øymar K, *et al.* Predictors of 24-h outcome in newborns in need of positive pressure ventilation at birth. *Resuscitation* 2018;129:1–5.
- Mduma E, Ersdal H, Svensen E, *et al.* Frequent brief on-site simulation training and reduction in 24-h neonatal mortality—an educational intervention study. *Resuscitation* 2015;93:1–7.
- Linde JE, Eilevstjønn J, Øymar K, *et al.* Feasibility of a prototype newborn resuscitation monitor to study transition at birth, measuring heart rate and ventilator parameters, an animal experimental study. *BMC Res Notes* 2017;10:235.
- American Academy of Pediatrics. Helping babies breathe. Available: <http://www.helpingbabiesbreathe.org/>
- Linde JE, Schulz J, Perlman JM, *et al.* Normal newborn heart rate in the first five minutes of life assessed by dry-electrode electrocardiography. *Neonatology* 2016;110:231–7.
- Gynecology ACoOa. ACOG Committee opinion 644: the Apgar score, 2015. Available: <https://www.acog.org/Clinical-Guidance-and-Publications/Committee-Opinions/Committee-on-Obstetric-Practice/The-Apgar-Score>
- Rabe-Hesketh S, Skrondal A. *Multilevel and longitudinal modelling using Stata*. Texas: StataCorp LP, 2012: 1. 134–7.
- Chalak LF, BARBER CA, HYNAN L, *et al.* End-Tidal CO₂ detection of an audible heart rate during neonatal cardiopulmonary resuscitation after asystole in asphyxiated piglets. *Pediatr Res* 2011;69:401–5.
- UN Inter-agency Group for Child Mortality Estimation. *Levels and trends in child mortality: report*. New York, 2017.
- O'Donnell CPF, Kamlin COF, Davis PG, *et al.* Interobserver variability of the 5-minute Apgar score. *J Pediatr* 2006;149:486–9.
- te Pas AB, Davis PG, Hooper SB, *et al.* From liquid to air: breathing after birth. *J Pediatr* 2008;152:607–11.
- van Vonderen JJ, Hooper SB, Krabbe VB, *et al.* Monitoring tidal volumes in preterm infants at birth: mask versus endotracheal ventilation. *Arch Dis Child Fetal Neonatal Ed* 2015;100:F43–6.
- Finer NN, Rich W, Wang C, *et al.* Airway obstruction during mask ventilation of very low birth weight infants during neonatal resuscitation. *Pediatrics* 2009;123:865–9.
- Schmolzer GM, Dawson JA, Kamlin COF, *et al.* Airway obstruction and gas leak during mask ventilation of preterm infants in the delivery room. *Arch Dis Child Fetal Neonatal Ed* 2011;96:F254–7.
- Boon AW, Milner AD, Hopkin IE. Physiological responses of the newborn infant to resuscitation. *Arch Dis Child* 1979;54:492–8.
- Kang LJ, Cheung P-Y, Pichler G, *et al.* Monitoring lung aeration during respiratory support in preterm infants at birth. *PLoS One* 2014;9:e102729.
- van Vonderen JJ, Roest AAW, Siew ML, *et al.* Measuring physiological changes during the transition to life after birth. *Neonatology* 2014;105:230–42.
- van Vonderen JJ, van Zanten HA, Schilleman K, *et al.* Cardiorespiratory monitoring during neonatal resuscitation for direct feedback and audit. *Front. Pediatr.* 2016;4(Suppl 1).
- Ersdal HL, Mduma E, Svensen E, *et al.* Birth asphyxia: a major cause of early neonatal mortality in a Tanzanian rural hospital. *Pediatrics* 2012;129:e1238–43.
- Schmölzer GM, te Pas AB, Davis PG, *et al.* Reducing lung injury during neonatal resuscitation of preterm infants. *J Pediatr* 2008;153:741–5.